

Investigation of the Interaction between Mucins and  $\beta$ -Lactoglobulin under Tribological Stress

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2	Investigation of the Interaction between Mucins and $\beta$ -Lactoglobulin under
3	Tribological Stress
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17	
18	Abstract
19	The interaction characteristics between mucins and beta-lactoglobulin (BLG) under tribological
20	stress were investigated by comparing the lubricity of mixed solutions of mucin-BLG with that of
21	neat protein solutions at compliant hydrophobic interfaces. Surface adsorption properties of the
22	proteins as characterized by bicinchoninic acid (BCA) assay revealed that both bovine submaxillary
23	mucin (BSM) and porcine gastric mucin (PGM) showed distinctly higher adsorbed masses
24	compared to BLG onto polydimethylsiloxane (PDMS) or polystyrene (PS) surfaces. The adsorbed

25 masses of the mixed protein solutions, namely BLG-BSM and BLG-PGM, reduced significantly, and BLG appeared to dominate the surface adsorption event, presumably due to the reduced 26 27 concentration of mucins and the Vroman effect. While pin-on-disk tribometry and mini-traction machine (MTM) were employed to provide the tribological contacts with varying contact pressure, 28 29 speed range, and slide/roll ratio, the dominant lubrication mechanism of the protein solutions was boundary lubrication. BLG-BSM mixture showed the highest level of degradation in the lubricity of 30 BSM at pH 5, although BLG-saliva interaction is known to degrade the lubricity most rapidly at 31 32 more acidic pH, such as at pH 3.5. More importantly, pH dependent lubricating properties of BLG-BSM mixed solutions appeared to be determined by competitive adsorption of the two proteins onto 33 the substrates, which suggests that they do not form as strong aggregates as BLG-saliva, especially 34 under tribological stress. 35

36

#### 37 **1. Introduction**

There has been growing interest in understanding food oral processing and digestion by applying 38 39 various techniques to achieve desired designing of food and pharmaceuticals with new ingredients 40 and interfacial structures (Lundin, Golding, & Wooster, 2008; McClements, Decker, & Park, 2009; 41 Singh, Ye, & Horne, 2009; Singh & Ye, 2013). A few studies have investigated food oral 42 processing by focusing on the interaction of food emulsions with saliva in the oral environment 43 (Vingerhoeds et al. 2005; van Aken, Vingerhoeds, & de Hoog, 2007; Silletti et al. 2007; Sarkar, Goh, & Singh, 2009). These studies have shown that either electrostatic interaction or hydrophobic 44 forces causes emulsion flocculation, aggregation, or aroma releasing, which are related to sensory 45 perception. Due to complexity of both food and saliva, the details of food-saliva interactions still 46 require further explanations. In particular, little information is available in literature on the 47 molecular-level interaction between constituents of food-saliva systems. 48

49	Recently, tribology has emerged as a new instrumental approach to investigate oral processing
50	of food emulsions in simulated oral environment (Meyer et al. 2011; Vardhanabhuti et al. 2011;
51	Chojnicka-Paszun, de Jongh, & de Kruif, 2012; Chen & Stokes, 2012; van Aken, 2013; Selway &
52	Stokes, 2013; Prakash, Tan, & Chen, 2013; Chen, Liu, & Prakash, 2014; Joyner Melito, Pernell, &
53	Daubert, 2014). In turn, this is often correlated with food's sensory perception (Meyer et al. 2011;
54	Vardhanabhuti et al. 2011; Chojnicka-Paszun, de Jongh, & de Kruif, 2012; Selway & Stokes, 2013;
55	Prakash, Tan, & Chen, 2013). Tribology is particularly useful for understanding the behavior of thin
56	films formed between two opposing surfaces where rheological and structural/mechanical
57	properties of food may no longer explain their behavior sufficiently.
58	In the present study, we attempted to apply tribological techniques to investigate the
59	interaction of $\beta$ -lactoglobulin (BLG) with mucins under tribological stress and how it affects their
60	lubricating properties. BLG is the major whey protein constituting > 50% of the total whey proteins
61	in bovine milk (Zúñiga, Tolkach, Kulozik, & Aguilera, 2010). BLG contains many charged groups,
62	therefore, its structure and properties are highly pH-dependent (Fang & Dalgleish, 1997). Mucins
63	are a family of large, extracellular glycoproteins (Bansil, Stanley, & LaMont, 1995; Svensson, &
64	Arnebrant, 2010) and are known to be chiefly responsible for the slipperiness of saliva (Tabak,
65	Kevine, Mandel, & Ellison, 1982; Berg, Lindh & Arnenrant, 2004). Apart from its functions in
66	biological systems, previous studies have shown facile adsorption and effective lubrication on
67	various engineering materials too (Lee, Müller, Rezwan, & Spencer, 2005; Yakubov, McColl,
68	Bongaerts & Ramsden, 2009; Nikogeorgos, Madsen, & Lee, 2014). The importance of
69	understanding the interaction characteristics between BLG and mucins is related to an ongoing
70	discussion on the origin of astringency. One of the most prevailing models is that astringents
71	interact with saliva to form aggregates to deplete the lubricant (saliva) from the tribological contacts
72	in the mouth (Rossetti, Bongaerts, Wantling, Stokes, & Williamson, 2009; Vardhanabhuti et al.,

73	2011). Recent applications of tribological techniques allowed for quantitative characterization of the
74	lubricating properties of the fluids involving saliva and BLG or other astringents. For example,
75	Vardhanabhuti et al. (2011) showed that addition of BLG into a soft tribological interface increased
76	the interfacial friction forces, yet at varying rates depending on pH. Aggregation of macromolecules
77	(BLG) with hydrogel (saliva) is, however, a complex process influenced by a number of
78	parameters. For example, among many types of proteins in saliva, which one(s) are involved in the
79	aggregation with BLG is not clear. Thus, it would be important and meaningful to investigate the
80	molecular-level interaction to deepen the understanding the interaction of saliva with whole food.
81	Moreover, despite relatively more active studies addressing the interactions of mucins with
82	polysaccharides (Qaqish, & Amiji, 1999; Menchicchi et al., 2014; Menchicchi et al., 2015), the
83	studies for the interaction of mucins with food proteins are much more limited.
84	We have chosen two types of mucins, namely, bovine submaxillary mucin (BSM) and porcine
85	gastric mucin (PGM), purchased from a commercial manufacturer (Sigma-Aldrich). The fact that
86	both mucins are highly relevant to food digestion process, yet to different organs, is the first reason
87	for comparing them. Additionally, in parallel with common structural features of the two mucins
88	(Bansil, Stanley, & LaMont, 1995; Sandberg, Blom, & Caldwell, 2009), reported differences in
89	their biophysical properties, especially the lubricating properties (Lee, Müller, Rezwan, & Spencer,
90	2005; Nikogeorgos, Madsen, & Lee, 2014), may lead to different interaction with BLG and
91	alteration in the lubricating properties.

# 93 **2. Materials and methods**

94 2.1 Sample preparation

95 BLG from bovine milk, BSM (Type I-S), and PGM (Type III) were purchased from Sigma-Aldrich

96 (Brøndby, Denmark), and were used as received. Protein solutions with the concentration of 1

97	mg/mL were prepared by dissolving in 10 mM phosphate buffered saline (PBS) solutions and were
98	used throughout the study. The pH values of the buffer solutions were adjusted to 7.4, 5, and 3 by
99	addition of HCl or NaOH. For the mixture of BLG and mucins, the two protein solutions were
100	mixed directly at the ratio of 1:1 (v:v) and the total protein concentrations were remained at either 1
101	mg/mL. Due to relatively weaker lubricating capabilities of PGM at 1 mg/mL (Lee, Müller,
102	Rezwan, & Spencer, 2005), PGM, BLG, and PGM-BLG mixed solutions were studied at 10 mg/mL
103	too.
104	
105	2.2 Zeta potential measurements
106	The zeta potential of the protein solutions was characterized with a laser (633 nm) Doppler
107	electrophoresis instrument (LDE; Zetasizer Nano ZS, Malvern, UK). Disposable cuvettes (model
108	DTS 1070) were used. At least five measurements were performed for each protein solution to
109	acquire statistically valid data.

111 *2.3 Bicinchoninic acid (BCA) assay* 

112 Surface adsorption properties of the proteins onto hydrophobic substrates were characterized by means of BCA protein qualification assay. This technique is based on the reduction of Cu<sup>2+</sup> to Cu<sup>+</sup> 113 in the presence of peptide bonds, and subsequent complex formation with BCA to form a purple-114 colored end product (Smith et al. 1985). The assay has been established to quantify proteins in bulk 115 116 solution, and recently, it was further customized to estimate the protein amount adsorbed on 117 surfaces (Sandberg, Mellina, Gelius, & Caldwell, 2009; Pakkanen, Madsen, & Lee, 2015). An 118 important assumption in this modified approach is that surface adsorbed proteins (peptide bonds) have the same reduction reactivity of converting Cu<sup>2+</sup> to Cu<sup>+</sup> with those in bulk solution. Thus, the 119 light absorbance by Cu<sup>+</sup>-BCA complex is proportional to the amount of the proteins even if the 120

proteins are surface-localized. Detailed procedures to acquire standard curves and the areal mass of 121 122 the sample proteins are provided in the Supplementary Information (Figure S1.) In this study, 123 standard curves were prepared for not only bovine serum albumin (BSA) as a general test protein, but also for all the proteins or protein mixtures at each condition, including concentration, pH, and 124 125 the choice of microtiter materials (see below). The absorbance of each protein sample was measured at 540 nm with an absorbance microplate reader (BioTek, ELx800 model). The 126 measurements were repeated three times for each sample for statistical evaluation. The microtiter 127 128 wells (GMBH+CO KG, Wertheim, Germany) were made of polystyrene (PS). While PS was not 129 used as a tribopair material, we assume that protein adsorption properties of the proteins onto PS would be similar with those onto polyoxymethlylene (POM), which was used as a tribopair 130 131 material. For the relevance of surface adsorption properties to tribological interfaces of poly(dimethylsiloxane) (PDMS), some microtiter wells were coated with a thin layer of PDMS. To 132 this end, a two-component silicone kit (Sylgard 184, Dow Corning) was employed. Base fluid and 133 crosslinker were mixed at the ratio of 10:1 (w/w). A small drop (ca. 20 µL) was added to each well 134 and cured in an oven at 80 °C overnight. It is noted that as standard curves were independently 135 136 obtained for PDM-coated wells too, thin PDMS coating on the absorbance does not affect the 137 adsorbed mass estimation.

138

# 139 2.4 Pin-on-disk tribometry

Lubricating properties of the protein solutions at sliding contacts were characterized by pin-on-disk tribometry (CSM, Peseux, Switzerland). In this approach, a loaded spherical pin is allowed to form a contact on a plane disk. The motor-driven rotation of the disk generates interfacial friction forces between the pin and the disk. The applied load is controlled by dead weight and the friction forces

145

defined from the relationship,  $\mu = F_{\text{friction}}/F_{\text{load}}$ .

146 PDMS was chosen as the tribopair for both pin (6 mm in diameter) and disk (30 mm in diameter and 5 mm in thickness). The pin and disk from PDMS were prepared with the PDMS kit 147 148 mentioned above as described by Nikogeorgos, Madsen, & Lee (2014). To ensure that the lubricated contacts were in the boundary lubrication regime, a low sliding speed (5 mm/s) was 149 selected under a 5 N or 2 N load, corresponding to the apparent maximum Hertzian contact pressure 150 151 of 0.6 or 0.4 MPa, respectively. The friction force data were collected for 100 rotations at room temperature (25 °C) and the tests were repeated multiple times for statistical evaluation. For each 152 153 measurement, a tribopair of PDMS-PDMS was used only once and discarded to avoid cross 154 contamination between measurements. As a control, a POM pin (6 mm in diameter) was employed to form a POM/PDMS interface under 5 N (apparent maximum Hertzian contact pressure of 0.9 155 MPa). The basic mechanical and surface properties of the tribopair materials are presented in Table 156 157 1.

generated during sliding contact are monitored by a strain gauge. The coefficient of friction,  $\mu$ , is

158

#### 159 *2.5 Mini traction machine (MTM)*

160 Lubrication properties of the protein solutions were characterized at mixed/rolling contacts in the higher speed regime by means of a mini-traction machine (MTM, PCS Instruments Ltd., UK) too. 161 162 Mixed rolling/sliding contacts are provided with MTM by independent rotation of ball and disk. The mean speed is defined as [ $|speed_{ball} - speed_{disk}|/2$ ]. The slide/roll ratio (SRR) is defined as SRR 163 =  $(|\text{speed}_{\text{ball}} - \text{speed}_{\text{disk}}|)/[(\text{speed}_{\text{ball}} + \text{speed}_{\text{disk}})/2] \times 100\%$ , where 0% SRR represents pure rolling 164 165 and 200% SRR represents pure sliding. In this study, SRR of 20% was employed in all measurements with varying mean speed between 10 mm/s to 1200 mm/s. Tests were conducted at 166 room temperature (25 °C) with the tribopair consisting of a POM ball and a PDMS disk. The PDMS 167

disks were prepared from the aforementioned two-component silicone kit (Sylgard 184, Dow Corning) as well. A thick PDMS slab (ca. 5 mm) was cast on top of a steel disk (ca. 5 mm) for each sample. POM balls were purchased from a supplier (19.05 mm (<sup>3</sup>/<sub>4</sub> inch) in diameter, Precision Plastic Ball Co., IL) and were used as received. For each measurement, a new PDMS disk was employed, whereas the same POM ball was used after cleaning with distilled water, ethanol, and sonication in distilled water for 5 min. A fixed load (2 N) was applied with the estimated Hertzian contact pressure of 0.3 MPa. Tests were repeated three times and the friction data were averaged.

176 **3. Results and discussion** 

### 177 *3.1 Zeta potentials*

178 In Figure 1, the zeta potentials of the protein solutions are presented as a function of pH. A zeta potential of near 0 mV was observed at pH 5 for BLG, which is indicative of near-zero net charge 179 180 and being close to the isoelectric point (IEP) of BLG. As expected, positive and negative zeta 181 potentials were measured when the pH was shifted to 3 and 7.4, respectively in agreement with the 182 study of Engelhardt et al. (2013). It is noted that despite a gradual decrease in the magnitude of 183 negative charges with decreasing pH, the zero zeta potentials of the mucins were not reached even 184 at pH 3, indicating that the IEPs of both mucins are lower than pH 3 (Lee, Müller, Rezwan, & Spencer, 2005; Sotres, Madsen, Arnebrant, & Lee, 2014). It is further to note that BSM displayed 185 186 more negative zeta potentials than PGM at all pH values due to higher abundance of negatively charged moieties in BSM, such as sialic acids (bound sialic acid 9 - 17% for BSM Type I-S and 0.5 187 - 1.5% for PGM Type III, Sigma Aldrich). 188 For the BLG-BSM mixture, the trend of the zeta potential changes according to pH change 189

appears to be similar to that of BSM itself, except for slightly less negative values. However, as theabsolute values of the zeta potential of BLG at pH 3 and 5 are much smaller than those of BSM at

these pHs, and as the zeta potentials of BLG and BSM are very similar to each other at pH 7.4, the interaction nature between BSM and BLG cannot be judged based on zeta potential data alone. The seemingly ignorable contribution of BLG to the zeta potential of BLG-PGM mixture at pH 5 could be also discussed in the same context. At pH 3 and 7.4, however, despite fairly different zeta potentials of BLG and PGM, their mixture showed nearly the same zeta potentials of PGM rather than intermediate ones, which signifies the dominance of the electrophoretic mobility of PGM in the mixed protein solutions.

199

#### 200 *3.2 Surface adsorption properties*

The adsorbed masses of the proteins per unit area, denoted as Γ, of the PDMS-coated microtiter
well surfaces are presented in Figure 2. It is noted that Figure 2(a) is for the data obtained from 1
mg/mL (all protein solutions) and Figure 2(b) is for those from 10 mg/mL (PGM, BLG, and BLG-

204 PGM mixture solutions only). The results for the PS microtiter wells were very similar and the

results are shown in Supplementary Information (Figure S3). A few noticeable features of the

adsorption behavior of mucins, BLG, and their mixtures are discussed as follows.

Firstly, the adsorbed masses of mucins were clearly higher than those of BLG under the same

208 conditions (concentration and pH). For instance, the  $\Gamma_{PGM}$  was ca. 3 mg/m<sup>2</sup> and  $\Gamma_{BSM}$  ranged ca. 2.0-

209 4.5 mg/m<sup>2</sup> from 1 mg/mL solutions for all pH values, whereas  $\Gamma_{BLG}$  ranged ca. 0.4-1.0 mg/m<sup>2</sup> only

210 (Figure 3). While the experimental approach employed in this study was markedly different from

211 more conventional optical approaches, the  $\Gamma$  values for mucins (Shi, & Caldwell, 2000; Lee,

212 Müller, Rezwan, & Spencer, 2005; Nikogeorgos, Madsen, & Lee, 2014) and BLG (Krisdhasima,

- 213 McGuire, & Sproull, 1992) onto hydrophobic surfaces are roughly in the same range, which
- supports the validity of BCA as a quantitative surface adsorption characterization technique. Given
- the adsorbed mass per unit area and the molecular weight of BSM (1.6 MDa, Shi, & Caldwell,

2000), PGM (1.25 MDa, Davies, & Viney, 2002), and BLG (18 kDa, Zúñiga, Tolkach, Kulozik, & 216 217 Aguilera, 2010), the number of protein molecules per unit area, or conversely, the surface area 218 occupied per single molecule could be estimated. If we further assume that this area is circular, its diameter,  $D_s$ , can be compared with the hydrodynamic diameter,  $D_h$ , of the proteins in a bulk 219 220 solution from literature (Durrer, Irache, Duchene, & Ponchel, 1995; Celebioglu et al., 2015). The results (Table 2) showed that the  $D_{s, BLG}$ , is comparable to  $D_{h, BLG}$  or smaller, whereas the  $D_{s, BSM}$  or 221  $D_{\rm s, PGM}$  is approximately only ca. 10-25% of their  $D_{\rm h}$  in bulk solution. This means that mucins are 222 223 not only higher than BLG in the adsorbed masses, but also adsorb onto the surfaces in a more 224 compact conformation due to a high flexibility of mucins to accommodate themselves in a narrow 225 space or a possibility to form multilayers. 226 Secondly, pH was observed to have an influence on the surface adsorption of both mucins and BLG. For instance, BSM showed higher adsorbed masses at acidic pHs than pH 7.4, in consistent 227 228 with a recent study by Sotres, Madsen, Arnebrant, & Lee (2014). This behavior is readily expected 229 from polyanionic characteristics of BSM and nonpolar characteristics of PDMS surface; adsorption 230 of polyanionic species onto nonpolar surfaces from aqueous environment inevitably leads to the 231 accumulation of charges on the surface and it act as a barrier to hamper further adsorption (Sotres, 232 Madsen, Arnebrant, & Lee, 2014). With decreasing pH, BSM starts to be protonated and the barrier can be diminished. The pH dependence of PGM for the adsorption onto PDMS at 1 mg/mL is much 233 234 weaker, and this is consistent with the fact that PGM carries less charged moieties as shown by the zeta potential measurements (Figure 1). However, at 10 mg/mL, PGM also showed a highest 235 236 adsorbed mass at pH 3 than at lower pHs, presumably due to the activation of the electrostatic 237 repulsion mechanism mentioned above. Adsorption of BLG onto PDMS surfaces showed a higher 238  $\Gamma_{BLG}$  values at pH 5 compared to pH 3 and 7.4, which could also be explained by the electrostatic repulsion model, as the zeta potential of BLG is nearly zero at pH 5 (Figure 1). 239

240 Thirdly, and most importantly, mixed protein solutions showed much lower  $\Gamma$  values than 241 those of respective mucins and comparable to BLG at each condition. While only a half of the 242 mucin concentration in the mixed protein solutions can be a first reason, this behavior could be ascribed also to the Vroman effect too (Vroman & Adams, 1969);Lassen & Malmsten, 1997; 243 244 Latour, 2008); as BLG is much smaller and lighter than the mucins, it is more mobile and can reach 245 the surface faster than the mucins in the early stage of adsorption ( $\leq 1$  hr in this study). Furthermore, as the weight/volume concentration of BLG and mucins were equal in the mixed 246 247 protein solutions, the number of BLG molecules overwhelms that of mucins due to much smaller molecular weight of BLG. Thus, BLG can readily dominate the initial surface adsorption.. 248 249 More importantly, the dominance of BLG in the surface adsorption from the BLG-mucin 250 mixture mentioned above implies that there is a large portion of "free" BLG molecules in the mixed 251 protein solutions, and that they participate in the surface adsorption process in competition with the 252 mucins. This is contradicting with a recent spectroscopic study on the interaction between BLG and 253 BSM (Celebioglu et al., 2015), in which the DLS measurements of the BLG-BSM mixture led to a 254 complete disappearance of the peak corresponding to free BLG molecules. This may be caused by 255 the substantially different light scattering sensitivity for the two types of molecules, i.e. BLG 256 molecules are not readily detectable when they are present together with much larger BSM molecules in a solution. It may also simply reflect a very weak interaction nature between BLG and 257 258 BSM even if they may form loose aggregates.

259

260 *3.3 Lubricating properties* 

In this study, two types of hydrophobic interfaces, namely PDMS-PDMS and POM-PDMS, were employed for the lubrication studies. Hydrophobic substrates were chosen as they may potentially mimic an oral mucosa membrane underneath mucus layers and facile adsorption of mucins onto the

substrate can complete an in-vitro oral mucosa model. More importantly, in order to assess the
boundary lubricating properties of the proteins, the substrates should effectively attract them onto
the surface in the first place, and thus hydrophobicity is a first demanded attribute as the tribopair.
POM and PDMS are though very different in their mechanical properties and surface roughness
(Table 2). Thus, without substantial changes in the tribological parameters, e.g. external load, these
two sliders provide significantly different contact pressure regimes on the opposing substrate.

270

## 271 3.3.1 Sliding contacts of soft-soft and smooth interface; pin-on-disk tribometry

Figure 3 shows the  $\mu$  values obtained from the sliding contacts of PDMS-PDMS interface as

273 lubricated by the protein solutions at (a) 1 mg/mL (all protein solutions) and (b) 10 mg/mL (PGM,

274 BLG, and BLG-PGM mixture solutions only) as characterized by pin-on-disk tribometry. Buffers

with three different pHs showed  $\mu$  values of 0.5-0.6 (Figure 3(a)). At 1 mg/mL concentration, the

BSM solutions displayed exceedingly superior lubricity. This is consistent with previous studies

showing effective boundary lubrication by BSM at a PDMS-PDMS interface, yet under much lower

load (Nikogeorgos, Madsen, & Lee, 2014). BSM showed higher  $\mu$  values at pH 3 ( $\mu \approx 0.2$ )

279 compared to pH 5 and 7.4 ( $\mu \approx 0.02$ ), for which the origin is not clearly understood yet. As the  $\Gamma_{BSM}$ 

values at pH 3 was comparable to those at pH 5 and higher than at pH 7.4 (Figure 2), this behavior

cannot be understood in view of surface coverage with BSM at varying pH. One possibility is that

charged BSM at pH 7 may lubricate more effectively due to charge-charge repulsion between theopposing surfaces.

# PGM solutions showed virtually ignorable lubricating effect, despite comparable adsorbed masses with BSM at the same concentration, 1 mg/mL (Figure 2). While the lubricity of the PGM solution improved at pH 3, in consistent with a former study (Lee, Müller, Rezwan, & Spencer,

287 2005), the  $\mu$  values were still somewhat higher than those of BSM at the same condition. It is also

noticeable that the lubricity of the PGM solutions at 10 mg/mL is not improving or even inferior to that of PGM at 1 mg/mL at pH 3 (Figure 3(b)). As a control, an experiment employing the 10 mg/mL PGM solution at pH 3 again showed low  $\mu$  values under a reduced load of 2 N (Figure 3(b)), the exceptionally high  $\mu$  values of 10 mg/mL PGM solutions at pH 3 under 5 N appear to be related to pressure-induced phenomena, such as bridging of PGM molecules between the two opposing PDMS surfaces and consequently high adhesive contacts.

294 The lubricating efficacy of BLG solutions was also observed to be poor. Although some variation in  $\mu$  values according to the pH change was observed, at both 1 mg/mL and 10 mg/mL 295 concentrations, the absolute  $\mu$  values were relatively high ( $\mu > 0.2$ ), indicating that this dependence 296 297 is of little importance. Insignificant lubricity of BLG is firstly resulting from the lack of distinct amphiphilicity, a structural feature required to stabilize the macromolecules on hydrophobic 298 299 substrates in aqueous environment. Relatively lower adsorbed masses and larger intermolecular 300 distances between BLG on PDMS surface (Table 2) suggest that a strong adhesion between PDMS 301 surfaces may be still active when PDMS-PDMS sliding contact is lubricated with BLG solutions.

302

## 303 *3.3.2 Sliding contacts of hard-soft and rough interface; pin-on-disk tribometry*

Figure 4 shows the  $\mu$  values obtained from POM-PDMS interface as lubricated by BSM solution at pH 7.4 or buffer solution under otherwise the same conditions with Figure 3. For a direct comparison, the  $\mu$  values from the PDMS-PDMS counterpart (Figure 3) are also presented. About two times higher  $\mu$  values observed from the POM-PDMS than the PDMS-PDMS interface in the buffer solutions is ascribed to the substantially higher surface roughness of the POM surface and consequently high local contact pressures (Table 1). Nevertheless, BSM solution displayed consistently more effective lubrication than BLG or the BLG-BSM mixture solutions. The

ineffective lubricity of the PGM solutions for the POM-PDMS interface was also consistent (datanot shown).

313

## 314 *3.3.3 Mixed rolling-sliding contacts of hard-soft and rough interface; MTM*

315 Figure 5 shows the  $\mu$  vs. speed plots obtained from the POM-PDMS tribopair lubricated with the 316 protein solutions at 1 mg/mL (a) at pH 3, (b) pH 5, and (c) pH 7.4, as characterized with MTM. The 317 results showed that all the protein solutions lowered the  $\mu$  values compared to the respective buffer 318 solutions (some missing  $\mu$  data points in the low-speed regime for the buffer solutions > 1), even 319 including PGM or BLG solutions, which were less lubricious in tribometer experiments. This is 320 probably due to more favorable conditions for lubrication, including higher speed, higher rolling 321 characteristics, and lower apparent contact pressure (0.3 MPa) for the MTM experiments. With 322 increasing mean speed, the  $\mu$  values of all the samples started to decrease, reaching as low as 0.03 323 for the case of BSM at pH 7.4. However, even in the highest speed regime, no characteristic up-turn of  $\mu$  values for elastohydrodynamic lubrication (EHL) (de Vincente, Stokes, & Spikes, 2005; 324 Nalam, Clasohm, Mashaghi, & Spencer, 2010) was observed. Thus, the dominant lubrication 325 mechanism is thought to be boundary and/or mixed lubrication without separation of the two 326 327 opposing surfaces by the fluids. Inability to activate EHL mechanism for this contact is largely related to high surface roughness of the POM ball (Table 1), which was also attributed to as a main 328 reason for higher friction forces for this pair in the pin-on-disk tribometry experiments (Figure 4). 329 330 The root-mean-square roughness (R<sub>q</sub>) of the POM ball and PDMS disk is  $659 \pm 179$  nm and  $1.6 \pm$ 331 0.3 nm, respectively. Therefore, the composite surface roughness of the POM-PDMS interface,

332  $R_{q,c} = \sqrt{R_{q,POM}^2 + R_{q,PDMS}^2}$ , is nearly identical with that of POM. Thus, for the activation of the

EHL mechanism, the lubricating film thickness should be at least 3 times larger than  $R_{q,c}$  (Røn, & 333 Lee 2014), i.e. ca. 2  $\mu$ m, which is not realistic, especially for aqueous lubrication. 334 335 Superior lubricity by the BSM solution to the other protein solutions, in particular at pH 7.4, 336 was observed in consistent with the pin-on-disk tribometry results (Figure 3 and 4). Due to the 337 degraded lubricity of BSM at pH 3, however, the relative difference in  $\mu$  values between the protein solutions became blurred, which also was consistent with the pin-on-disk tribometry data (Figure 338 339 3). In fact, the  $\mu$  values for the PGM solutions were slightly lower than those of BSM at pH 3, but 340 this difference became much smaller in the high-speed regime. The data obtained from 10 mg/mL 341 solutions of PGM or BLG-PGM (Supplementary Information, Figure S2) were nearly indistinguishable from those obtained from 1 mg/mL in Figure 5. 342 343 3.3.4 Surface adsorption properties and lubricity; BSM vs PGM 344 A strong contrast in the lubricity between BSM and PGM at PDMS-PDMS sliding interface 345 346 remains elusive to be understood; both mucins are known to be large in molecular weight and 347 comparable to each other (Sandberg, Blom, & Caldwell, 2009). Both are heavily glycosylated in the central region to similar extents, and are proposed to be adsorbing onto hydrophobic surfaces from 348 349 water via hydrophobic interaction with unglycosylated C- and N-terminal regions. The adsorbed 350 masses onto PDMS surface were also fairly comparable for BSM and PGM as shown from the 351 same concentration, 1 mg/mL, in this study (Figure 2). It should be noted that the aqueous lubrication by adsorption of amphiphilic macromolecules 352 onto hydrophobic surfaces is achieved essentially by hydration of the hydrophobic surfaces and 353 354 removal of hydrophobic adhesion between the two opposing surfaces (Lee, & Spencer, 2005). For 355 mucins, this is achieved by respective role of unglycosylated terminal regions acting as an anchor

356 onto the surface and the glycosylated central region acting to recruit water into the interface as

mentioned above. Critically important for effective lubrication is to sustain the lubricating layer, i.e. 357 mucin film, under persistently applied tribostress, not just to adsorb in high amount under initial 358 359 tribostress-free condition. Thus, the adsorbed mass determined in the absence of tribostress (Figure 2) provides only a first indication for lubricity. Another related point to note is that as the adsorption 360 361 of mucins onto hydrophobic surfaces is achieved mainly via hydrophobic interaction, its binding 362 strength is not strong enough to withstand the tribostress as a monolayer coating. For example, a 363 recent study demonstrated that a monolayer coating of BSM on PDMS surface immersed in buffer 364 solution, i.e. without excess BSM in solution, showed an immediate loss of lubricity upon sliding against a PDMS slider and a gradual increase of  $\mu$  with increasing rotation on a sliding track 365 366 (Nikogeorgos, Madsen, & Lee, 2014). Thus, effective lubrication by a BSM solution at PDMS-PDMS or POM-PDMS interfaces is enabled by continuous re-establishment of the lubricating film 367 368 under tribostress involving the cycles of adsorption-desorption-readsorption of BSM molecules. Thus, the superior lubricity of BSM to PGM should be related to many other factors than the 369 adsorbed mass itself, such as BSM's superior binding strength onto the surface, more optimized 370 371 conformation to hydrate the surface, as well as faster convection to the surface to re-form the 372 lubricating films, or the combination thereof.

In order to visualize the relationship between the lubrication efficacy and the surface 373 adsorption properties of the proteins in this study, their adsorbed masses,  $\Gamma$ , are plotted against  $\mu$ 374 375 values obtained from the pin-on-disk tribometry in Figure 6. Because of somewhat extreme 376 behavior of PGM and its mixture with BLG at 10 mg/mL, only the data obtained from 1 mg/mL 377 protein solutions are displayed. In Figure 6, as the BSM data set lies in the "right-bottom" quadrant, it reflects the case where high adsorbed mass is directly correlated with effective lubrication. The  $\mu$ 378 379 vs. Γ plots also display that the relatively higher friction of BSM at pH 3 is not due to the reduced adsorbed mass at that pH condition. PGM, being placed in the "right-upper" quadrant, clearly 380

demonstrates the case where high adsorbed mass is not sufficient for effective boundary lubrication.
Lastly, the location of BLG in the "upper-left" quadrant in the plot suggests that the poor adsorption
onto PDMS surface is probably the primary reason for its poor boundary lubrication properties.

## 385 *3.3.5 Lubricating properties of BLG-mucin mixtures*

Distinctively different lubricating properties of BSM and BLG make it most interesting to explore the effect of mixing the two proteins. As mentioned earlier, this is interesting largely because a previous study by Vardhanabhuti et al. (2011) reported that the addition of a BLG solution to the PDMS-PDMS interface, lubricated by human saliva film, led to a rapid loss of lubricity at an acidic pH (3.5), but at a much slower pace at pH 7 or 5.

391 The relationship in the change of the adsorbed mass and lubricity upon mixing BLG and BSM 392 could be clearly manifested in the  $\mu$  vs.  $\Gamma$  plots in Figure 6. Basically, as a group, the BLG-BSM 393 data set is shifted leftwards, yet without shifting upwards with respect to the BSM data set, suggesting that the lubricity of BSM is generally maintained despite significantly reduced adsorbed 394 395 masses upon mixing with BLG. In more detail, at pH 7.4, a substantial reduction in the adsorbed 396 mass is accompanied with only a slight degradation of BSM's lubricity upon mixing with BLG. If 397 the reduced surface adsorption is related to the competitive adsorption of BLG, this observation is surprising because, under persistently applied tribostress, molecules that adsorb quicker, i.e. BLG, 398 399 should dominate the tribological interface. A fairly well sustained lubricity of the BLG-BSM mixture compared to the neat BSM solution suggests that BSM rather dominates the tribological 400 401 properties of the mixture at this pH. One possible explanation is that as the adsorption of BLG onto 402 PDMS surface tends to leave the ample PDMS surface uncovered (see the section 3.2), BSM can 403 readily overlay onto the surface that is pre-occupied with BLG at pH 7.4 and still effectively 404 lubricate the tribological interface. At pH 5, however, a drastic reduction in both the adsorbed mass

405	and lubricity of BLG-BSM mixture compared BSM is observed. This is related to more facile
406	adsorption of BLG onto PDMS surface at pH 5 than at pH 3 or 7.4; the adsorbed mass of BLG at
407	pH 5 was roughly twice those at pH 3 and 7.4 (Figure 2). In turn, this can be attributed to the
408	electrostatic neutrality of BLG at this pH (Figure 1) and the absence of electrostatic repulsion
409	between BLG molecules in the surface adsorption process. Thus, the dominance of BLG at the
410	tribological interface, i.e. clearly degraded lubricity of BLG-BSM mixture compared to BSM, can
411	be intensified at pH 5. At pH 3, a reduction in the adsorbed mass without degrading lubricity is
412	observed upon mixing BSM with BLG, similarly with pH 7.4. However, as the $\mu$ values of BLG
413	and BSM are similar to each other, the dominance of BLG at the tribological interface can be
414	suggested only based on the significantly reduced adsorbed mass.
415	Overall, a strong pH dependence of the lubricating properties of BLG-BSM at the PDMS-
416	PDMS interface, which can be related to the reported pH dependence of the lubricating properties
417	of BLG-saliva interaction, was confirmed even on a molecular level interaction. However, more
418	detailed trends are very different in the interaction of BLG-saliva vs. BLG-BSM. Firstly, for the
419	former, strong interaction of BLG with saliva (Vingerhoeds, Blijdenstein, Zoet, & van Aken, 2005)
420	or mucosa (Withers, Cook, Methven, Gosney, & Khutoryanskiy, 2013) has well been established
421	and it formulates the ground for the rapid depletion of saliva films from the tribological interface at
422	pH 3.5. Meanwhile, for the mixed BLG-BSM solution at 1 mg/mL concentration, competitive
423	adsorption between them onto the tribological interface and its dependence on pH appears mainly
424	responsible for varying lubricity according to pH change. This means, however, that BLG and
425	mucins do not formulate tightly bound aggregates in the mixture solution. Secondly, while rapid
426	degradation of lubricity was observed only at pH 3.5 for the BLG-saliva interaction, the degraded
427	lubricity was most prominent at pH 5 for the BLG-BSM interaction, yet much weaker at pH 7.4 or
428	pH 3. Again, this is due to that the main cause for the degrading lubricity of BLG-BSM mixed

solution is competitive adsorption onto the tribological interface rather than strong aggregationbetween them.

For the mixtures of BLG-PGM, as the lubricity of BLG or PGM, as well as the mixed
solution of BLG-PGM, is equally poor, the tribology data alone do not provide conclusive
information on the interaction between BLG and PGM. Meanwhile, Figure 6 shows that the net
effect of mixing BLG and PGM is featured with substantially decreased adsorbed masses compared
to the neat PGM solutions. Thus, it can be also suggested that BLG dominates the tribological
interface for BLG-PGM mixture.

437

# 438 4. Conclusions

439 In this study, we have investigated the molecular-level interaction between mucins and BLG by means of tribological approaches according to mucin type, solution pH, and protein concentration. 440 Hydrophobic interfaces, namely PDMS-PDMS and POM-PDMS, were employed for feasible 441 442 adsorption of the proteins and consequent possibility of assessment of the boundary lubricating 443 properties. Surface adsorption properties of the proteins by BCA assay revealed that both mucins 444 adsorbed onto the hydrophobic substrates in a large amount to form either highly compact layers or 445 multilayers, whereas BLG appeared to adsorb without interfering with neighboring molecules or 446 even by partly exposing bare substrates. This difference was firstly related to generally more 447 effective lubricating properties of mucins, in particular BSM, compared to BLG. Nevertheless, nearly ignorable lubricating effect by PGM, despite its facile surface adsorption, suggests that other 448 449 parameters than adsorbed masses play a significant role to impart superior lubricity of BSM to 450 PGM or BLG. While both pin-on-disk tribometry and MTM were employed to provide the tribological contacts with different contact pressure, speed range, and slide/roll ratio, the 451 dominating lubrication mechanism by the protein solution was boundary lubrication. Surface 452

adsorption and lubricating properties of mixed protein solutions, such as BLG-BSM and BLG-453 PGM, with respect to neat protein solutions were of prime interest as it can be compared with the 454 455 well-known role of BLG as astringency to form a complex with saliva and rapidly deplete from the tribological interface at acidic pH (3.5, for example). Even in the absence of tribostress, the 456 457 adsorbed masses of the mixed protein solutions reduced significantly, and BLG appeared to dominate the surface adsorption event, presumably due to the reduced concentration of mucins as 458 459 well as the Vroman effect. Nevertheless, excellent lubricity was still observed at pH 7.4 and BSM 460 apparently dominated the tribological interface, which highlights the excellent lubricating capabilities of BSM. Although being still relatively more lubricious than the other proteins, the 461 462 BLG-BSM mixture showed the highest level of degradation in the lubricity of BSM at pH 5, which 463 contrasts the case of BLG-saliva interaction. This is due to that instead of strong aggregation, as in BLG-saliva, the lubricating properties of BLG-BSM are determined by competitive adsorption of 464 465 the two proteins onto substrates. Most importantly, these observations further suggest that BLG and 466 BSM molecules do not form strong aggregates, especially under tribological stress. PGM's 467 intrinsically weaker lubricity remained largely unchanged even in the interaction with BLG. 468

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- 590

592	Table 1.										
		Young's modulus	Poisson ratio	Surface	Static water						
		(MPa)		roughness	contact angle						
				(nm)	(°)						
	PDMS	2	0.5	$1.6\pm0.3$	$105.6\pm.2$						
	POM	3100	0.35	$659 \pm 179$	$84.8\pm2.9$						

# 596 Table 2.

Samples	Adsorbed mass (mg/m <sup>2</sup> )			<i>A</i> , Area per protein molecule (nm <sup>2</sup> )		D <sub>s</sub> , Distance between protein molecule on surface (nm)		$D_{ m s}/D_{ m h}$				
pН	3	5	7.4	3	5	7.4	3	5	7.4	3	5	7.4
BSM	2.03	4.54	2.11	1307.6	585.2	1258.0	40.8	27.3	40.0	0.25	0.17	0.24
PGM	2.81	2.94	3.07	737.3	706.9	674.5	30.6	30.0	17.0	0.14	0.13	0.10
BLG	0.49	1.10	0.38	62.0	27.7	79.8	62.0	27.7	79.8	1.37	0.91	1.55