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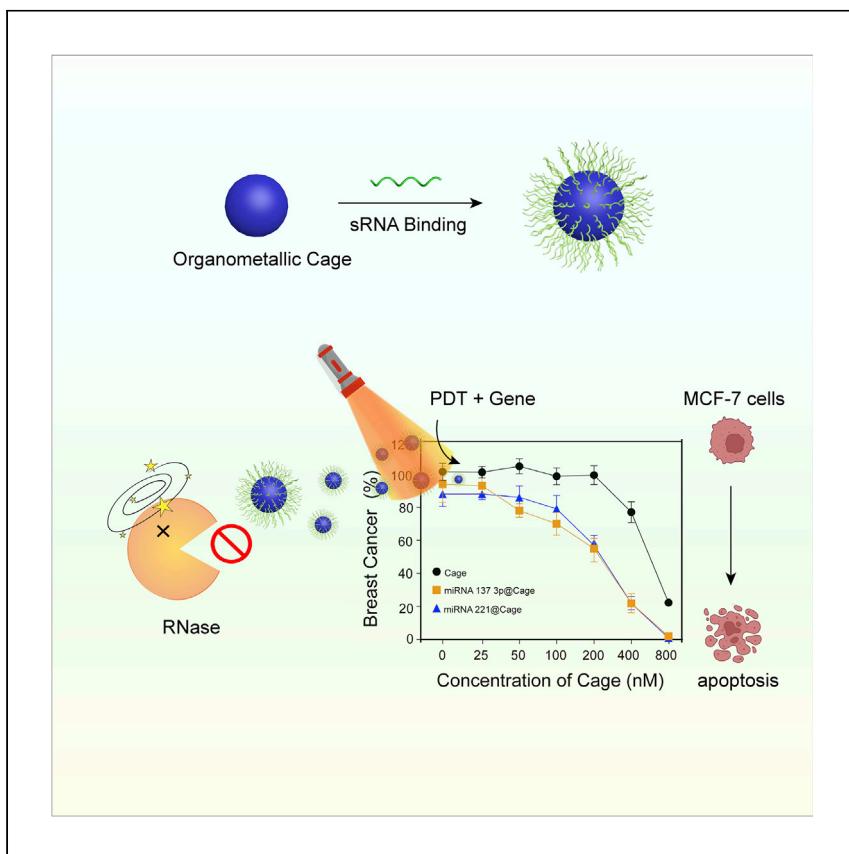
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Article

Small RNA stabilization via non-covalent binding with a metalloporphyrin nanocage to accomplish synergistic gene and photodynamic therapy



Small RNAs are regarded as attractive therapeutic agents, but biodegradation severely limits their application. Herein, Weiguang et al. report on small RNAs binding to metalloporphyrin cages, significantly protecting RNA against degradation and facilitating synergistic gene regulation and photodynamic therapy for killing breast cancer cells.

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Highlights

Small RNAs efficiently bind to metalloporphyrin cages via non-covalent interactions

Strong binding significantly enhances the small RNA human serum stability

The platform is used for synergistic gene regulation and photodynamic therapy

Article

Small RNA stabilization via non-covalent binding with a metalloporphyrin nanocage to accomplish synergistic gene and photodynamic therapy

Weiguang Jin,¹ Xin Li,² Gael Clergeaud,² Roslyn M. Ray,³ Marie Karen Tracy Hong Lin,⁴ Thomas Lars Andresen,² Charlotte Held Gotfredsen,¹ Martin Nielsen,¹ Kira Astakhova,^{1,*} and Katrine Qvortrup^{1,5,*}

SUMMARY

Small RNAs (sRNAs) have emerged as attractive therapeutic agents due to their gene-editing and -regulatory properties. However, their application is severely limited by their relatively short circulation half-lives. Herein, we report a strategy binding sRNA with metalloporphyrin cages that leads to a significant protection of sRNA against RNase degradation and increased half-lives. Nuclear magnetic resonance (NMR) titration of nucleosides and nucleotides demonstrates that π -stacking and electrostatic interactions contribute to the sRNA binding, which occurs on the external surface of the nanocage. Moreover, the cage binding promotes sRNA internalization, and the sRNAs maintain genetic activity after release in an acidic intracellular environment. Taking advantage of the photodynamic properties of the cage, the nanosystem shows efficient *in vitro* cell killing through gene regulation and photodynamic effects, providing evidence for its therapeutic potential in breast cancer treatment. We envision the proposed strategy may provide new insight for the development of organometallic cage-based sRNA delivery vehicles.

INTRODUCTION

Small RNA (sRNA), defined as RNA with 18–30 nucleotides,¹ is therapeutically important for a range of human diseases, including cancer. In CRISPR-Cas9 gene editing, for example, the use of guide RNA (gRNA) functions as a guide for targeting enzymes, which is a key strategy to minimize off-target effects and optimize efficiency of the system.² In addition, endogenous sRNA molecules, such as microRNA (miRNA), have been linked to many diseases,³ especially cancer,⁴ as their biological action results in the overexpression of oncogenic proteins or the down-regulation of tumor-suppressor proteins.⁵ Introducing exogenous miRNA that inhibit gene expression of overexpressed miRNA or balance down-regulated miRNA are promising gene therapies.⁶ Therapeutic applications of sRNA are, however, severely limited due to their susceptibility to degradation by prevalent ribonucleases in the bloodstream and cell environment,⁷ which results in short circulation half-lives of less than 2 min.⁸ To overcome the instability of RNA, the use of RNA-loaded nanoparticles has received increasing attention due to their nanoscale size and functional surface.⁹ A broad range of nanomaterials have been investigated, including metallic nanoparticles,¹⁰ liposomes,¹¹ and polymers.¹²

Learning from the nanoparticle-RNA formulations, metal-organic cages (MOCs) are attractive nanocomponents for sRNA binding and stabilization due to their unique

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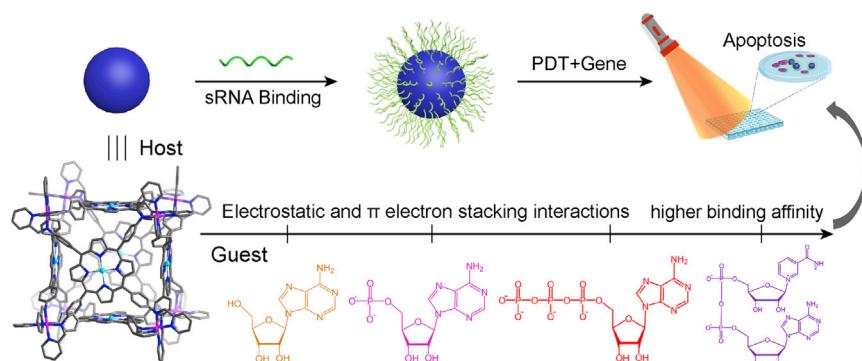
structural characteristics. Driven by self-assembly of molecular components, MOCs are rationally constructed as highly symmetrical and discrete supramolecular polyhedrons, which facilitate their nanoscale dimensional distribution.¹³ In addition, these structurally well-defined MOCs allow the incorporation of desired functional groups to modify the structural characteristics, resulting in expeditious tuning of key features, including solubility as well as binding properties, with the ability to bind a wide range of guest molecules through relevant non-covalent interactions.¹⁴ Meanwhile, intrinsic relatively weak and dynamic non-covalent host-guest supramolecular binding allows the convenient reattachment of guest molecules at a low energy cost.¹⁵ Compared with the traditional metal complex, the MOCs arouse extensive interest in supramolecular host-guest interaction due to their large cavity and surface area.^{16,17} Guest encapsulation using the interior cavity is the most popular strategy to explore and utilize the supramolecular binding ability of MOCs.^{18,19} This interior binding generally needs a suitable internal environment within the cavity to match the desired trapped guest molecules.²⁰ While this is effective for the binding of small-molecule guests, it does not allow encapsulation and stabilization of larger biomolecules.^{21–23} To further expand the application of MOCs, the binding of guest molecules to the exterior surface is an attractive strategy.^{24,25} Ward and co-workers recently showed strong binding between anionic aromatic fluorophores and the exterior surface of cationic MOCs.²⁶

Due to the above-mentioned advantages of host-guest interactions, the binding of DNA molecules with $\text{Ni}^{II}{}_4\text{L}_6$ ²⁷ and $\text{Fe}^{II}{}_4\text{L}_4$ tetrahedral cages^{28,29} was recently reported, protecting DNA from nuclease-mediated degradation. Compared with DNA, reports describing sRNA binding with MOCs are limited. The higher instability of RNA compared with DNA, resulting from a nucleophilic attack on the phosphorus atom attacked by the adjacent ribose 2' hydroxyl groups, pose a major challenge when designing RNA binders.³⁰ Given that DNA deoxynucleotides and RNA ribonucleotides are similar structural motifs, the pioneering DNA recognition studies offer a positive reflection to our proposal of sRNA binding and stabilization with MOCs.

Recent studies have shown that a combination of sRNA, especially miRNA, transfection, and photodynamic therapy (PDT) has a strong anti-cancer effect.^{31–33} Various MOC-based nanostructures were utilized as photosensitizers to generate reactive oxygen species (ROS),¹⁸ but, to our knowledge, there is no report on sRNA-bound MOC structures for sRNA stabilization, miRNA activity, and PDT. Given the strong properties of the porphyrin unit as a photosensitizer,³⁴ we hypothesized that a $\text{Fe}^{II}{}_8\text{L}_6$ metalloporphyrin structure could show strong sRNA binding and stabilization while having good anti-cancer properties through miRNA-mediated gene regulation and MOC-based PDT.

Herein, we present the preparation and characterization of two isostructural metalloporphyrin cubic cages (**Scheme 1**) and demonstrate their ability to bind sRNA, hereby significantly enhancing sRNA resistance against RNase degradation and stability in human serum. Nuclear magnetic resonance (NMR) titration of relevant nucleoside and nucleotide biomolecules demonstrate that electrostatic and π -stacking interactions contribute to the binding. The encapsulation of coronene inside the cage has a negligible effect on dinucleotide and sRNA binding, confirming that the binding only occurred on the external surface of the cage. Moreover, the bound sRNA can be released under acidic conditions, mimicking the cancer intracellular environment.

As a proof-of-concept study, we selected breast cancer MCF-7 cells to demonstrate that the cage significantly promoted the internalization of the bound sRNA and



Scheme 1. Small RNA surface binding with metalloporphyrin cage through electrostatic and π -stacking interactions, resulting in significant stability against ribonuclease degradation and a synergistic therapy involving gene regulation and cage-based PDT for breast cancer treatment (cage 1 \cdot SO₄ contains zinc-porphyrin motifs, while its isostructural cage 2 \cdot SO₄ contains free-base porphyrin faces)

maintenance of its biological activity after release from the cage. Importantly, the sRNA@cage nanocomplex facilitated synergistic therapeutic behavior combining miRNA regulation and PDT properties, efficiently killing MCF-7 cells. Overall, our findings demonstrated the feasibility of reversible surface binding for the preparation of MOC-based sRNA carriers and their potential use as a synergistic enhancer for cancer therapies using a combination of gene regulation and PDT. We envision that the results may create new insight and inspiration for the use of MOC-based sRNA delivery vehicles.

RESULTS AND DISCUSSION

Characterization of the sRNA binding with cages

Cage 1 \cdot SO₄ and cage 2 \cdot SO₄ were synthesized through subcomponent self-assembly³⁵ (Section S2 in the supplemental experimental procedures) and, rewardingly, were found to display both good water solubility and stability under physiological conditions as seen from their time-dependent UV-visible (UV-vis) (Figure S8) and NMR (Figure S9) spectroscopy. In addition, dynamic light scattering (DLS) indicated that cages disperse at nanoscale in water (Figures S10 and S11). The ILK-1 CRISP gRNA, designed to knock out the integrin-linked kinase encoding gene,³⁶ was used for initial binding studies with equal concentrations of cage. The cationic cages 1 \cdot SO₄ and 2 \cdot SO₄ bind the innate negatively charged sRNA through electrostatic interactions, as the corresponding zeta potential of cages changed from positive to negative after mixing with equal concentrations of sRNA (Figure S12). Meanwhile, the single negative charge signal of complexes indicated that the sRNA was located on the external surface of the cages (Section S4 in the supplemental experimental procedures).³⁷ Efficient binding was also seen from ILK-1 titration, which induced a red shift of the UV-vis absorbance spectra of cage 1 \cdot SO₄ (Figure 1B).³⁸ When we extended the binding study to other sRNA, miRNA 221 and miRNA 137 3p, similar phenomena were seen in both zeta potentials and UV-vis absorbance (Sections S4 and S5 in the supplemental experimental procedures).

Denaturing PAGE was also used to study the binding. Since the positively charged cage acts as a counter ion to the negatively charged RNA, the intensity and mobility of the RNA bands on the gel will be affected by the cage concentration.³⁹ As shown in Figure 1C, the cage was not absorbed into the gel due to charge repulsion but instead was driven into the running buffer,²⁹ resulting in a black lane 1, while the

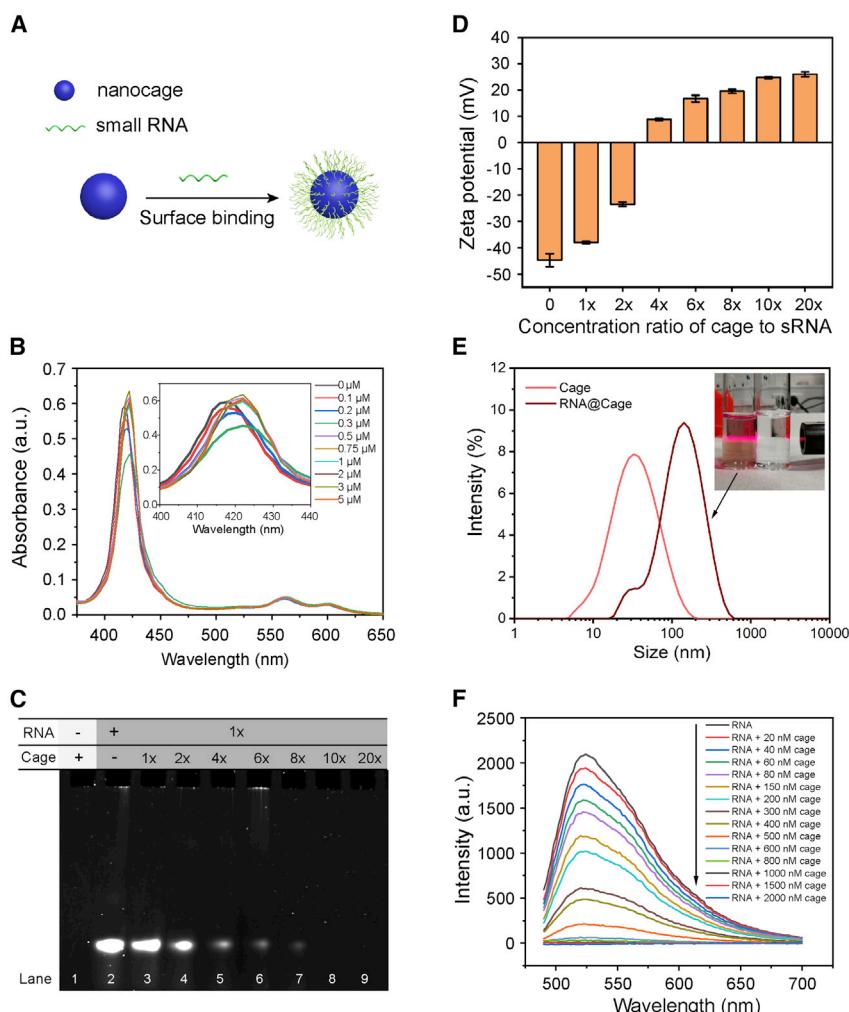


Figure 1. Characterization of the sRNA binding with cages

- (A) Cartoon showing the formation of sRNA@cage.
- (B) UV-vis absorbance spectra of cage 1-SO₄ with ILK-1 titration.
- (C) PAGE image of naked cage 1-SO₄ (lane 1), naked miRNA 137 3p (lane 2), and the corresponding complexes of miRNA 137 3p@cage 1-SO₄ with various concentration ratios (lanes 3–9).
- (D) Average zeta potential value of miRNA 137 3p without and with cage 1-SO₄ at various concentration ratios. The data are presented as means \pm SDs ($n = 3$).
- (E) DLS particle size distribution of bare cage 1-SO₄ and miRNA137 3p@cage 1-SO₄. The inserted picture shows the Tyndall effect of the miRNA137 3p@cage 1-SO₄ transparent brown solution (left), while nothing is observed in the water (right). The molar ratio of cage:RNA was kept at 10:1.
- (F) Fluorescent quenching of 100 nM FAM-labeled ILK-1 dependent on cage 1-SO₄ concentration.

signal of naked miRNA 137 3p is seen in lane 2 upon applying the electrophoresis voltage. The corresponding PAGE band intensity of the complexes gradually decreased and disappeared when the cage concentration reached 10 equiv to miRNA 137 3p (Figure 1C, lane 8), which is ascribed to the zeta potential of mixtures gradually increasing and changing from negative to positive (Figure 1D), further indicating complete binding. The same gel phenomena were observed for ILK-1 and miRNA 221, where signals also disappeared in the presence of 10 equiv of cage (Figures S28 and S29). As expected, the binding increased the DLS particle size, and the complex formed a transparent suspension with typical Tyndall effect (Figure 1E). Both sRNA@cage 1-SO₄ and sRNA@cage 2-SO₄ showed negligible

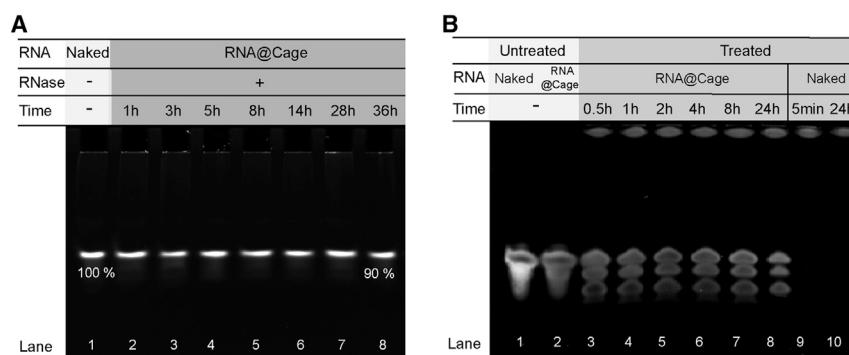


Figure 2. Cage binding enhances sRNA stability

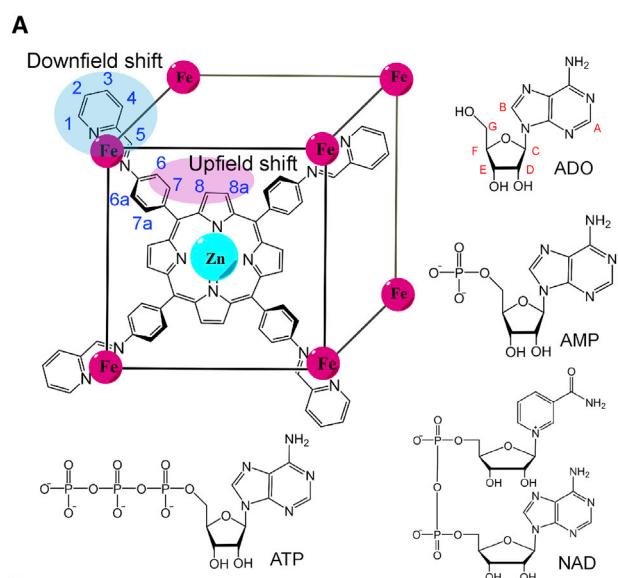
RNA stability analyzed by PAGE measurement of miRNA 137 3p@cage 1·SO₄ incubated with RNase (A) and ILK-1 with or without cage 1·SO₄ in human serum (B) at different times (the concentration ratio of cage 1·SO₄ to RNA was kept as 10:1; the percentage of RNA was analyzed by the band intensity, while the naked RNA at lane 1 was used as reference).

changes in the time-dependent UV-vis spectra and the DLS particle size distribution over the course of 48 h, thereby demonstrating the stability of the complexes in solution (Figures S30 and S31). The transmission electron microscopy (TEM) image showed that the amorphous RNA was aggregated around the cage nanoparticles (Figure S32B), which could also confirm that the RNA was bound to the outer surface of the cage nanoparticles, although the vacuum drying measurement conditions resulted in the loss of morphology of sRNA@cage.

To gain more insights into the interaction, we studied the fluorescent behavior of the 6-carboxyfluorescein (FAM)-labeled sRNA under cage titration. The emission of FAM-sRNA can be effectively quenched by cage through fluorescence resonance energy transfer.⁴⁰ As shown in Figure 1F, an increase in the concentration of cage 1·SO₄ gradually weakened the fluorescence emission of the FAM-labeled ILK-1 gRNA and led to complete quenching with 10 equiv cage, which is consistent with PAGE binding rate. In addition, similar effects on the fluorescence were seen upon titration of cage 1·SO₄ with FAM-labeled miRNA 137 3p and cage 2·SO₄ with FAM-labeled ILK-1 (Figure S33). Importantly, no obvious fluorescent change of the free dye was observed when it was mixed with the cages (Figure S34A), and the respective components of the cages had no significant quenching effect on the FAM-RNA fluorescence (Figure S34B). These results clearly illustrate that the quenching originates from the interaction of the cage with the sRNA rather than with the FAM molecule and that only the fully assembled cage structures allow effective interaction.

Cage binding enhances sRNA stability

Encouraged by the binding behavior, we investigated the potential of the cage for sRNA stabilization via PAGE. As RNase is a common enzyme causing RNA hydrolysis in biological microenvironments,⁴¹ we first evaluated the stability of sRNA with and without cage binding under RNase digestion. No PAGE band was observed from miRNA 137 3p after 1 h (Figure S36), which indicates complete degradation. On the contrary, the band corresponding to the miRNA 137 3p was well retained from the samples containing cage 1·SO₄ (Figure 2A), and approximately 90% of intact miRNA 137 3p was observed after 36 h. We further investigated the stability of sRNA in human serum. Notably, these experiments also showed a significant resistance to degradation of ILK-1 gRNA when complexed to the cage. The presence of intact ILK-1 could be observed after 24 h of exposure to serum, while the naked



B

Host	Guest	Binding constant / M ⁻¹
Cage 1·SO ₄	ADO	(2.35 ± 0.05) × 10 ²
	AMP	(5.25 ± 0.07) × 10 ²
	ATP	(7.62 ± 0.12) × 10 ²
	NAD	(1.681 ± 0.007) × 10 ³
Cage 2·SO ₄	NAD	(1.094 ± 0.008) × 10 ³
cor c cage 2·SO ₄	NAD	(1.087 ± 0.012) × 10 ³

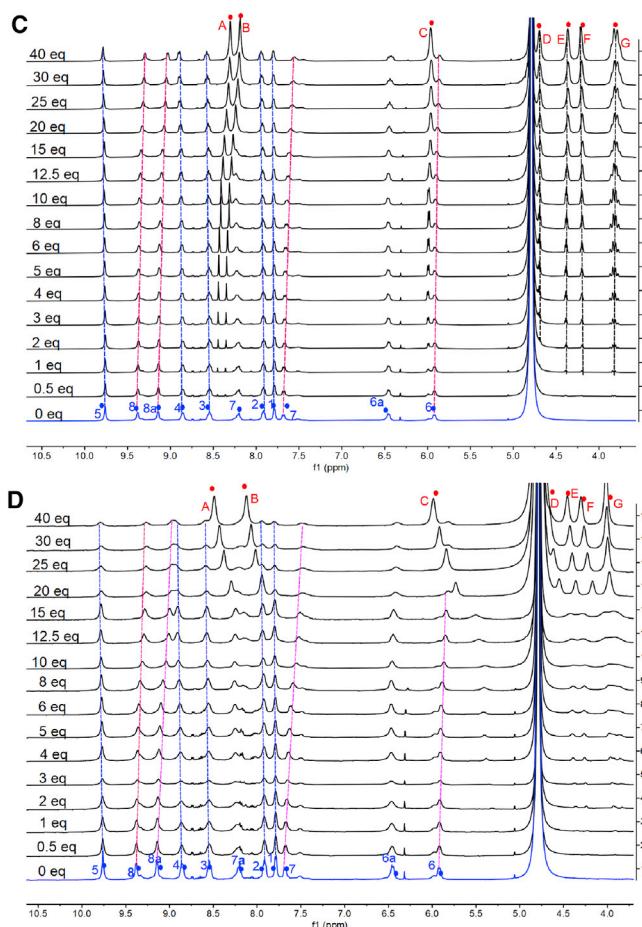


Figure 3. Binding mechanism investigated by nucleoside and nucleotide NMR titration

(A and B) The prospective nucleoside and nucleotide NMR titration (A) and their affinity constants with cages (B).

(C and D) The titration of ADO (C) and AMP (D) with cage 1·SO₄ monitored by ¹H NMR, respectively (blue and pink lines denote down-field and up-field shifts, respectively).

ILK-1 rapidly degraded within 5 min (Figures 2B, S37, and S38). These results clearly demonstrate that the cage has the ability to protect sRNA against RNase biodegradation and improve the stability in human serum.

Binding mechanism study

To explore the binding mechanism, selective nucleoside and nucleotide biomolecules were employed for NMR titration experiments (Figure 3A). Aliquots of cage 1·SO₄ were added to the respective biomolecule solution with different concentrations, and the corresponding spectra were recorded sequentially. Clear changes in chemical shift ($|\Delta\delta| > 0.01$ ppm) of proton resonances corresponding to both cage and guests were observed during titration, indicating that the cage can bind both nucleoside and nucleotide biomolecules.⁴² Meanwhile, the corresponding calculated binding constants of the biomolecules illustrate their different affinity with cage (Figure 3B). Based on the ¹H NMR results of adenosine (ADO) titration (Figure 3C), the signals of nucleobase showed a gradual up-field shift, while the ribose remained unchanged during the titration. Meanwhile, the central porphyrin ring of the cage gradually shifted toward upfield, while an opposite trend occurred in the pyridine ring. Therefore, we speculated that there is a π-stacking interaction

between the ADO nucleobase and the central porphyrin component of the cage,⁴³ triggering an electron transfer from the terminal site of cage to its central part.

Cage 1·SO₄ also showed a change in chemical shift upon titration with ADO monophosphate (AMP), but the nucleotide behaved completely different compared with the ADO (Figure 3D). The signal of the ribose moiety experienced a gradual down-field shift, while signals remained unchanged in ADO, and the base unit shifted downfield. A significant Δδ (0.02–2.31 ppm) was observed in the ³¹P NMR titration spectrum of AMP (Figure S44), and its significantly higher association affinity demonstrated that the phosphate also participates in the interaction, which led to its different ¹H NMR behavior compared with ADO. This proposed interaction was confirmed by studying the binding between ADO triphosphate (ATP) and cage 1·SO₄. Similarly, all signals of the ATP guest undergo a down-field shift in both ¹H NMR and ³¹P NMR spectra (Figures S46 and S47). Moreover, the cage 1·SO₄ exhibited a higher binding affinity for ATP compared with AMP (Figure S48).

To further verify this speculative mechanism, the complexation of nicotinamide adenine dinucleotide (NAD) was studied. As expected, all signals of NAD gradually shifted downfield (Figure S49), and the binding constants indicate that cage 1·SO₄ binds NAD with high affinity (Figure S50). When replacing cage 1·SO₄ with cage 2·SO₄, the same interaction with NAD was observed (Figure S51). The only difference between these two interactions is that the binding coefficient of cage 1·SO₄ is higher than that of cage 2·SO₄ (Figure S52), which reinforces the hypothesis that electrostatic interactions dominate the binding, as cage 1·SO₄ has a higher positive electron potential compared with cage 2·SO₄. Moreover, the ¹H NMR signals of cage 2·SO₄ also showed a gradual up-field shift in central porphyrin ring along with a down-field shift in its terminal pyridine, which occurred in the ¹H NMR of cage 1·SO₄ with all selected nucleoside and nucleotide biomolecules, further demonstrating that a similar π-stacking interaction occurred. Therefore, the two main interactions that contribute to the cage-sRNA binding are concluded to be π stacking between sRNA unpaired base units and the central porphyrin of the cage as well as electrostatic interactions between the negatively charged sRNA and the positively charged cage, with our experiments indicating that the latter dominates the binding.

Verification of outside surface binding

To confirm that the biomolecule is bound to the outer surface of the cage structure instead of entering its cavity, we introduced a coronene molecule into the cage 2·SO₄ to fill its cavity, forming corCage 2·SO₄ (Section S12 in the supplemental experimental procedures). Coronene was chosen as a relevant model structure due to its electrical neutrality in addition to the previously reported successful encapsulation of coronene in cage 2·OTI.⁴⁴ Afterward, NMR titration experiments were performed with biomolecule NAD and corCage 2·SO₄ in an aqueous solution to identify whether the coronene affects the nucleotide binding (Figure 4A). Although the cavity was occupied, the result of ¹H NMR was similar to studies of the empty cage 2·SO₄, with an insignificant change in binding affinity (Figure S55). Meanwhile, the encapsulated coronene showed an up-field shift arising from the higher shielding effect induced by the NAD binding on the external surface of cage, indicating the coronene maintained inside the cage during the nucleotide binding.

In addition to the NMR titration experiment, we also performed a fluorescence assay to investigate the interaction between corCage 2·SO₄ and FAM-labeled sRNA to evaluate the effect of coronene encapsulation on sRNA binding. Similar to the empty

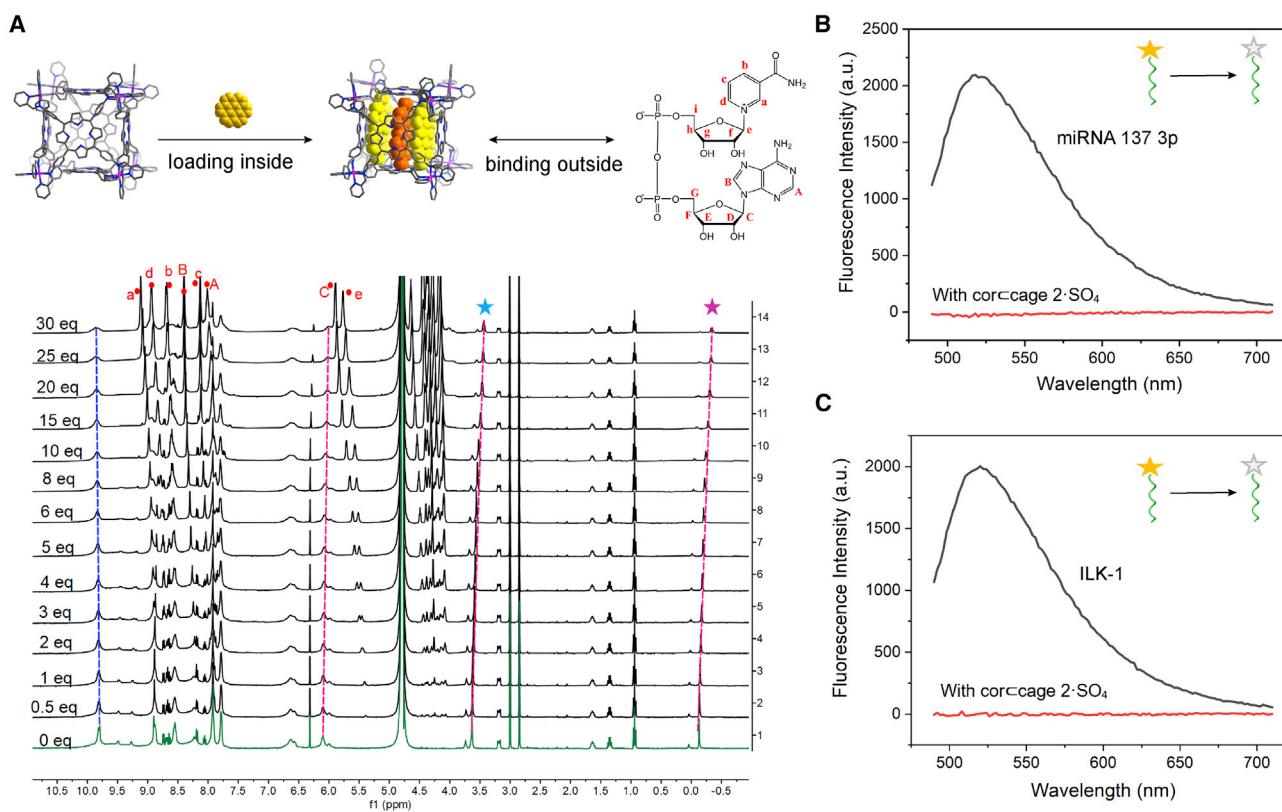


Figure 4. Verification of sRNA binding with the outside surface of cage

(A) NAD nucleotide NMR titration with corC cage 2·SO₄ (blue and pink lines denote down-field and up-field shifts, respectively; the signal of trapped coronene, which is marked with blue and pink stars, experience gradual up-field shift during the titration).
(B and C) The complex of corC cage 2·SO₄ led to fluorescence quench of FAM-labeled miRNA 137 3p (B) and FAM-labeled ILK-1 sequences (C).

cage, the FAM-labeled miRNA 137 3p and ILK-1 were quenched by corC cage 2·SO₄, respectively, indicating that the encapsulation of coronene has negligible effects on sRNA binding (Figures 4B and 4C). Given that the RNA sequence has a significantly larger molecular size than NAD, this also indicates that the bound RNA was located on the outer surface of the cage. According to the fact that sRNA only interacts with the exterior surface of the cage, we can conclude successful surface binding. Meanwhile, we also envision that the unexplored interior cavity could be used for other small-molecule deliveries, which will be investigated in the future.

RNA release

As sRNA has been proven to bind the exterior surface of the cage through non-covalent host-guest supramolecular binding, we next studied the sRNA release properties. The miRNA 137 3p@cage 2·SO₄ (ratios: 1:5 and 1:10) complexes were incubated in both neutral and acidic aqueous solutions (pH 5) for 1 h, followed by PAGE analysis. As shown in Figure 5A, the PAGE signal (lanes 4–7) of the intact miRNA 137 3p was clearly observed after incubation in acidic solution, mimicking the acidic intracellular environment of cancer. This demonstrates that the miRNA 137 3p can be released from the cage in an acidic environment. In contrast, when incubated with up to 10 equiv of the cage in neutral buffer (lane 3), no band corresponding to released sRNA was observed. These results also demonstrate retained strong RNA and cage binding under neutral conditions, which mimic circulating conditions. EDTA

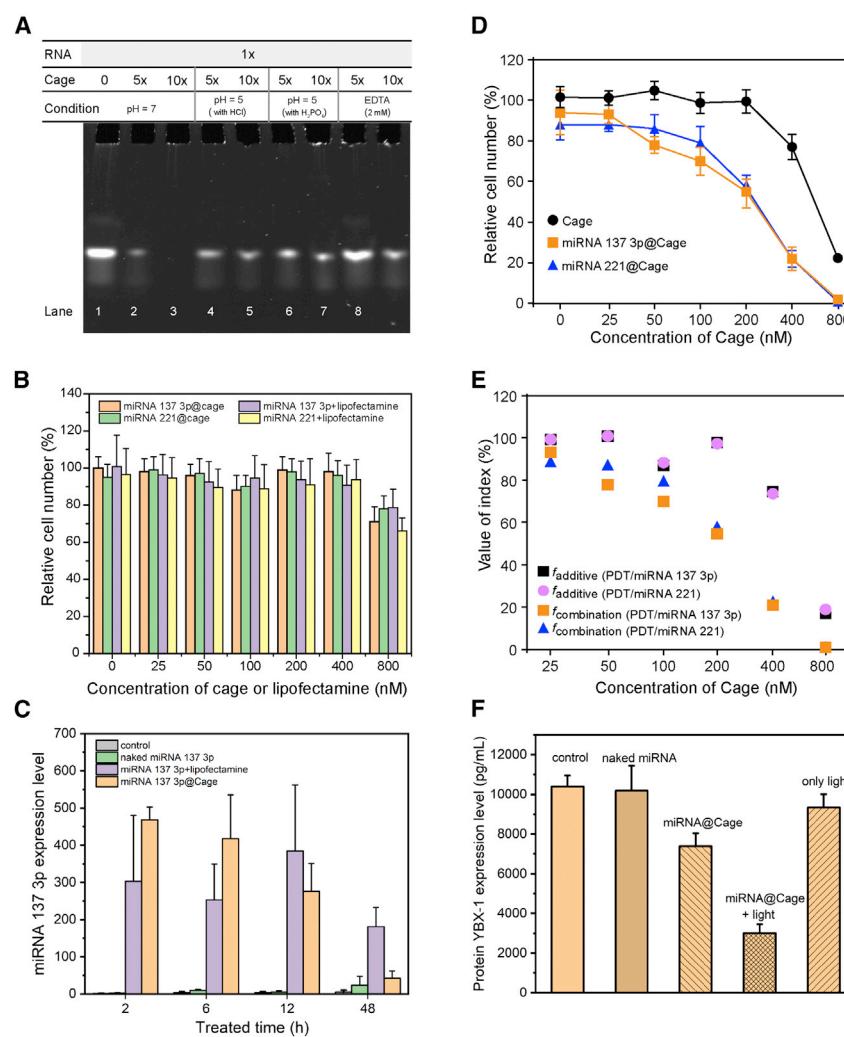


Figure 5. RNA release and the synergistic gene regulation and photodynamic effect for therapeutic potential in breast cancer treatment

(A) The release of miRNA 137 3p from the complex of miRNA 137 3p@ cage 2·SO₄ measured by PAGE (the naked miRNA 137 3p at lane 1 is used as reference).

(B) Cytotoxicity of miRNAs with lipofectamine and miRNA@cage 2·SO₄ in MCF-7 cells at various concentrations for 48 h in the dark. The concentration ratio of lipofectamine:RNA or cage:RNA was 10:1. The data are presented as means \pm SDs ($n = 3$).

(C) miRNA 137 3p level inside MCF-7 cells after treatment with different samples, which were prepared with the same miRNA amount with 10 equiv of lipofectamine or cage 2·SO₄. The data are presented as means \pm SDs ($n = 3$).

(D) Cytotoxicity of cage 2·SO₄ and miRNA@cage 2·SO₄ in MCF-7 cells with light irradiation at various concentrations. The cells were exposed to a 416 nm wavelength light for 30 min during the 48 h treatment period, and the molar ratio of cage:RNA was maintained at 10:1. The data are presented as means \pm SDs ($n = 3$).

(E) Compared with the f_{additive} , the significantly smaller $f_{\text{combination}}$ at various concentrations indicates a synergistic gene regulation and photodynamic effect of miRNA@cage 2·SO₄.

(F) Protein YBX-1 expression in the MCF-7 cells after treatment. The concentration of miRNA 137 3p was kept at the same for all sample preparations. The data are presented as means \pm SDs ($n = 3$).

was also found to facilitate the RNA release (lanes 8 and 9). Also, exposing the miRNA 221@cage 2·SO₄ to acidic conditions promoted the release of miRNA 221 from the corresponding binding complex (Figure S56). We attribute disassembly of the cage in the acidic environment to impair sRNA binding, leading to sRNA release.²⁹

MCF-7 cancer cell treatment

Having provided evidence for the release mechanism, we examined the potential of the sRNA@cage 2·SO₄ in cancer treatment. Considering that miRNA 221 and miRNA 137 3p are involved in the genetic dysregulation in breast cancer,^{45,46} we studied MCF-7 cell viability with naked miRNA 137 3p, miRNA 221, and their respective cage complexes. After 48 h incubation in the dark, no obvious cytotoxicity was observed from naked miRNAs at various concentrations ([Figure S57](#)), which was ascribed to miRNA degradation and inefficient intracellular transfection. In contrast, a slight reduction in cell count was observed in the presence of miRNA 221@cage 2·SO₄ and miRNA 137 3p@cage 2·SO₄ ([Figure 5B](#)), which was highly similar to the data from the corresponding miRNAs transfected with lipofectamine, a commercial transfection reagent. To confirm that the cage can promote miRNA internalization, qPCR was performed to quantify the amount of miRNA 137 3p after treatment of MCF-7 cells with miRNA, miRNA transfected with lipofectamine, and miRNA 137 3p@cage 2·SO₄, respectively, at 2, 6, 12, and 48 h ([Figure 5C](#)). After 2 h treatment, no miRNA 137 3p was found in the cell treated with naked miRNA, but a significant miRNA amount was detected when miRNA 137 3p was transfected with both lipofectamine and cage 2·SO₄. The miRNA 137 3p@cage 2·SO₄ transfected the highest amount of RNA at 2 h, with a gradual decrease of miRNA 137 3p levels observed over treatment time, which may be attributed to the release of bound RNA and subsequent relevant biodegradation in the cancer cells. The gradual decreasing trend of the RNA amount with transfection time was also observed when using lipofectamine. Rewardingly, these findings clearly demonstrate that cage binding can efficiently enhance the cellular uptake of RNA and retain the biological activity of the RNA. In addition, no anti-proliferation effect was observed in healthy control cells, human dermal fibroblasts (HDFs), after 48 h incubation with cage 2·SO₄ and the complexes ([Figure S58](#)), which reveals their biocompatibility.

Given the organic porphyrin component of the cage is a highly effective photosensitizer, the synergistic effect of PDT and the gene-regulating effect was studied for miRNA 221@cage 2·SO₄ and miRNA 137 3p@cage 2·SO₄. The cage was found to be stable under light irradiation at a 416 nm wavelength as the signal of cage 2·SO₄ in NMR and UV-vis spectra remained unchanged ([Figures S59](#) and [S60](#)). Meanwhile, the generation of ROS was detected in cage 2·SO₄ and its miRNA complex solution under irradiation, showing their potential PDT properties ([Figure S61](#)). The cytotoxicity assay of MCF-7 cells with the treatment of cage 2·SO₄ and the miRNA complexes were applied to assess the synergistic therapy. As shown as [Figure 5D](#), cage 2·SO₄ induced MCF-7 cell death with an IC₅₀ value of 563.6 nM. Importantly, miRNA 221@cage 2·SO₄ and miRNA 137 3p@cage 2·SO₄ showed a significant enhanced cellular apoptosis, leading to full cell death at 800 nM. Their respective IC₅₀ values were estimated as 204.8 and 178.5 nM. Comparing their additive index (f_{additive}), the respective smaller combination index (f_{combination}) clearly shows a synergistic effect of the gene regulation and PDT ([Figure 5E](#)).

To further understand the synergistic effect of PDT and miRNA gene regulation, we studied the expression of the potential targeted protein using enzyme-linked immunosorbent assay (ELISA). MCF-7 cells were treated with naked miRNA 137 3p, miRNA 137 3p@cage 2·SO₄, or miRNA 137 3p@cage 2·SO₄ with 30 min 416 nm light irradiation. Also, a control with only light irradiation was included. Restoring miRNA 137 3p expression is reported to inhibit the overexpression of target Y-box binding protein 1 (YBX1) and suppress cancer growth;^{46,47} thus, we compared the expression level of YBX1 after 48 h treatment. As shown as [Figure 5F](#), due to the lack of protection and transfection, the naked miRNA was unable to affect the YBX1

expression, with no apparent difference compared with untreated MCF-7 cells. In contrast, a reduction of the YBX1 expression was observed with miRNA 137 3p@cage 2·SO₄, further demonstrating that the RNA retained activity after cage binding. Importantly, better inhibition of protein expression was observed with miRNA 137 3p@cage 2·SO₄ with 30 min light irradiation, while the only light irradiation condition led to a negligible down-regulation of YBX1 expression as well as no decrease in cell viability in HDF and MCF-7 cells (Figure S62). These results show that the PDT of the cages and the miRNA activity give rise to a decrease in the expression of YBX1 in a synergistic manner to kill the MCF-7 cells. While the synergistic anti-cancer effect of the PDT and gene therapy have been previously reported,^{48–52} it is notable that our work shows, for the first time, the combination of PDT and miRNA gene regulation of a sRNA@cage nanocomplex, thus expanding its potential biological application.

The above findings clearly demonstrate the ability of Fe^{II}₈L₆ cages to strongly bind sRNA through non-covalent interactions, significantly enhancing the stability of the sRNA against RNase degradation in serum. Importantly, only the fully assembled cages were found to effectively bind sRNA, as no significant interaction was seen with its structural components. The binding mechanism was investigated by NMR titration with relevant biomolecules, showing that the cage interacts with sRNA through a combination of π-stacking and electrostatic interactions, which is consistent with the structural characteristics of the cage consisting of a highly π-electron-dense and positively charged framework. The encapsulation of coronene inside the cage has a negligible effect on dinucleotide and sRNA binding, proving that the sRNA only binds the outer surface of the cage. Moreover, the cage binding promoted the sRNA internalization, while the bound sRNA maintained activity after release in the acidic intracellular environment. Using biologically relevant miRNA sequences, the potential of the cage as a synergistic treatment, combining gene regulation and PDT, was demonstrated in MCF-7 breast cancer cells. Encouraged by these results, we envision that the proposed surface binding strategy through non-covalent chemistry can be generalized to MOCs for sRNA delivery regardless of interior pore, which allows other small-molecule loading for co-delivery. We also believe that the presented MOC-based nanostructure provides new insight for the development of MOC-based sRNA delivery vehicles and new promising candidates for synergistic gene regulation and photodynamic tumor therapy.

EXPERIMENTAL PROCEDURES

Resource availability

Lead contact

Further information and requests for resources should be directed to and will be fulfilled by the lead contact, Katrine Qvortrup (kaqvo@kemi.dtu.dk).

Materials availability

This study did not generate new unique materials. Requests for any materials used in the manuscript are available from the [lead contact](#) upon reasonable request.

Data and code availability

Correspondence and requests for materials or data used in the manuscript are available from the [lead contact](#) upon reasonable request.

SUPPLEMENTAL INFORMATION

Supplemental information can be found online at <https://doi.org/10.1016/j.xcrp.2022.101187>.

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AUTHOR CONTRIBUTIONS

K.A. and K.Q. conceived the project; W.J. designed and performed the experiments; X.L. conducted the cytotoxicity assay; W.J. and X.L. analyzed data; R.M.R. conducted qPCR; M.K.T.H.L. measured the TEM imaging; C.H.G. provided expertise and feedback for NMR experiments; G.C., T.L.A., M.N., K.A., and K.Q. provided resources; W.J. and K.Q. drafted the manuscript; and all authors edited this manuscript.

DECLARATION OF INTERESTS

The authors declare no competing interests.

INCLUSION AND DIVERSITY

We support inclusive, diverse, and equitable conduct of research.

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