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Improved Focusing Method for 3-D Imaging using 
Row–Column-Addressed 2-D Arrays

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Abstract—A row–column-addressed (RCA) 2-D array can be interpreted as two orthogonal 1-D arrays. By transmitting with row elements and receiving the echoes through column elements or vice versa, a rectilinear volume in front of the array can be beamformed. Since the transmit and receive 1-D arrays are orthogonal to each other, only one-way focusing is possible in each transmit or receive plane. For applications, where the scatterers are sparse, e.g., in micro-bubble tracking, to improve the focusing this study suggests to multiply the envelope data received by the row elements, when transmitting with columns as well as the data received by the column elements when transmitting with rows. By using the proposed method it is possible to achieve two-way focusing in both transmit and receive directions.

II. FOCUSING WITH ROW-COLUMN ADDRESSED ARRAYS

The vertical and horizontal arrays of the RCA 2-D array can each steer the transmit ultrasound beam in one direction. When the horizontal array is used as a transmit array, it can steer the transmit angle in the z-x plane, and at the same time the vertical array is receiving in the z-y plane. After the sequence has completed, the two arrays switch function, and now the vertical array is used as a transmit array and the horizontal array is receiving. This leads to two identical volumes of the rectilinear region in front of the array. However, at each point only one-way focusing is achievable either in transmit or receive. The pulse-echo pressure fields for both sequences using a rectangular apodization at each point (x, y, z), i.e., $\Phi_{\text{fa}}(x,y,z)$ and $\Phi_{\text{fa}}(x,y,z)$, can be estimated by: [12]

$$\Phi_{\text{fa}}(x,y,z) = \frac{L_x}{\lambda} \sqrt{\frac{\rho}{\lambda^2}} e^{i \frac{\pi}{4}} \text{sinc}\left( \frac{L_x}{\lambda z} \right) \frac{L_x}{\lambda} \sqrt{\frac{\rho}{\lambda^2}} e^{i \frac{\pi}{4}} \text{sinc}\left( \frac{L_y}{\lambda z} \right),$$

(1)

$$\Phi_{\text{fa}}(x,y,z) = \frac{L_x}{\lambda} \sqrt{\frac{\rho}{\lambda^2}} e^{i \frac{\pi}{4}} \text{sinc}\left( \frac{L_x}{\lambda z} \right) \frac{L_x}{\lambda} \sqrt{\frac{\rho}{\lambda^2}} e^{i \frac{\pi}{4}} \text{sinc}\left( \frac{L_y}{\lambda z} \right),$$

(2)

where $L_x$ and $L_y$ are the length of each row and column element, $\rho_u$ is the mass density of the medium, and $\lambda$ is the sound wavelength. In a similar way the pulse-echo pressure field for an FA 2-D array can be estimated by:

$$\Phi_{\text{fa}}(x,y,z) = \left( \frac{L_x}{\lambda} \sqrt{\frac{\rho}{\lambda^2}} e^{i \frac{\pi}{4}} \text{sinc}\left( \frac{L_x}{\lambda z} \right) \frac{L_x}{\lambda} \sqrt{\frac{\rho}{\lambda^2}} e^{i \frac{\pi}{4}} \text{sinc}\left( \frac{L_y}{\lambda z} \right) \right)^2.$$  (3)

The reflected pressure field from the scattering pattern, $\chi(x,y,z)$, using the RCA and FA 2-D arrays, indicated by $P_{\text{fa}}(x,y,z)$, $P_{\text{fa}}(x,y,z)$, and $P_{\text{fa}}(x,y,z)$, can be formulated as:
Two synthetic aperture imaging (SAI) sequences were designed for imaging down to 14 cm of depth. They utilize 62 single element transmissions on each row as well as column element. In both sequences the echoes are collected with all the perpendicular elements.

B. Measurement Setup

Measurements are acquired with one prototyped and fully integrated 2-D RCA PZT probe. It is connected to the experimental ultrasound scanner SARUS [13]. The measured RF signals are beamformed using a MATLAB (MathWorks Inc., Massachusetts, USA) implementation of delay-and-sum (DAS) beamformer for RCA 2-D arrays [8]. The transducer’s parameters are shown in Table I. For a speed of sound of 1540 m/s, 182 µs is required to acquire a single image line to a depth of 14 cm. For 124 emissions this is equivalent to a volume rate of 44 Hz.

A geometrical copper wire phantom, where wires located at different depths with 1 cm spacing, was used as line targets, to evaluate the imaging performance of the proposed focusing method, in terms of FWHM and cystic resolution [11] as a function of depth.

IV. RESULTS

Fig. 2 illustrates three cross planes (Azimuth, Elevation, and C-plane) of the simulated PSFs for different imaging sequences. When using only row elements in transmit and receive, although a two-way focusing is achieved in the elevation plane, no focusing can be made on the lateral plane (Fig. 2.a). Using only column elements for transmit and receive, achieves the same result but on the other perpendicular plane (Fig. 2.b). On the other hand, when using the row elements in transmit and column elements in receive or vice versa, a one-way focusing can be achieved in both lateral and elevation planes (Fig. 2.c and Fig. 2.d). Multiplying the last two PSFs generates a two-way focused PSF in both lateral and elevation planes (Fig. 2.e).

In (7) the reflectivity amplitude of the scatterer can not be preserved, and therefore to account for that, before multiplying the two volumes, each has to be equalized with its maximum value.

Measured examples of the proposed focusing scheme is illustrated in Fig. 3 and Fig. 4. In Fig. 3a and Fig. 4a by transmitting with row elements and receiving the RF-data with column elements a volume in front of the array is imaged. In Fig. 3b and Fig. 4b the proposed method is applied by multiplying the envelope data acquired, when using row elements for transmission and column elements for reception.

\[
P_{\text{TXRC}}(x,y,z) = \Phi_{\text{TXRC}}(x,y,z) \ast \chi(x,y,z), \quad (4)
\]

\[
P_{\text{RXRP}}(x,y,z) = \Phi_{\text{RXRP}}(x,y,z) \ast \chi(x,y,z), \quad (5)
\]

\[
P_{\text{FA}}(x,y,z) = \Phi_{\text{FA}}(x,y,z) \ast \chi(x,y,z). \quad (6)
\]

If the scattering pattern is a point-like target that can be represented as a Dirac function, then:

\[
P_{\text{FA}}(x,y,z) = P_{\text{TXRC}}(x,y,z) \cdot P_{\text{RXRP}}(x,y,z). \quad (7)
\]
Fig. 2. A scatterer is located at 20 mm depth in front of the array. Three cross planes (Azimuth, Elevation, and C-plane) of the simulated PSFs for different imaging sequences are shown, when: (a) transmitting and receiving with row elements, (b) transmitting and receiving with column elements, (c) transmitting with row and receiving with column elements, (d) transmitting with column and receiving with row elements, and (e) transmitting with both row and column, and receiving with both row and column elements. The C-planes are at depth of 20 mm.

Fig. 3. Two elevation planes of a wire grid phantom are shown. (a): transmitting with row elements and receiving the RF-data with column elements, (b): the proposed method.

Fig. 4. Two elevation planes of a hollow cyst phantom are shown. (a): transmitting with row elements and receiving the RF-data with column elements, (b): the proposed method.
and vice versa. The effectiveness of the proposed method is more visible on the wire grid phantom, since the point targets are not overlapping, which is not the case for the cyst phantom. The calculated FWHM and cystic resolution [11], over the middle column of wires, are illustrated in Fig. 5b and Fig. 5a.

Another advantage of the proposed method, is the possibility to lower the number of emissions to acquire a volume. In conventional row–column imaging, in order to have the same spatial resolution in each dimension, we required to transmit with all the transmit elements which is equal to the number of receive elements. However by using the proposed method we do not need necessarily transmit the same number of times as the number of received elements. This is due to the increase in the resolution by using the new method. Therefore, the number of transmissions in each dimension can be decreased.

V. CONCLUSION

This study presented a method for increasing the spatial resolution of the RCA 2-D arrays and validated it based on simulation and phantom measurements. The proposed method has the limitation to be only applicable to point-like targets, which are distributed sparsely. Compared with the conventional row–column imaging, the proposed method lowers the frame rate, as it requires to acquire each volume region in front of the array two times with the perpendicular 1-D arrays. The method assumes that the scatterers are not moving, however for moving targets a motion compensation method has to be sought. Further study has to be carried out to prove its applicability in ultrasound imaging by tracking micro-bubbles.

REFERENCES